

The logo features a stylized yellow human figure in a running pose, positioned over a green square with a white cross. The text 'Anatomical' is above 'Human' and '3D' is to the right of 'Human'.

methods of segmentation and modeling of the hip

Jérôme Schmid

Pula, Italy 21/05/2008

- Hip anatomy and clinical context
- Musculoskeletal modeling and problematic
- Acquisition
- Segmentation
- Results and applications

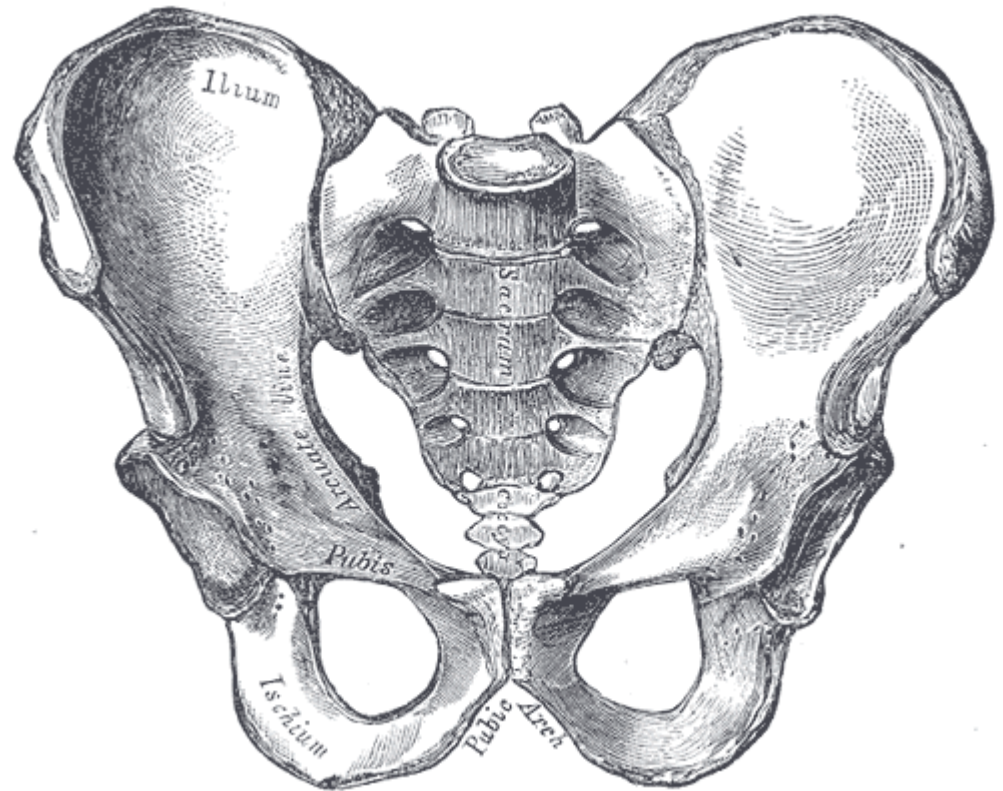
Hip Anatomy (1/5)



■ Bones

▣ Pelvis

- Hip bone (ilium, ischium and pubis)
- Coccyx
- Sacrum



Henry Gray, 1918, Anatomy of the human Body

Hip Anatomy (1/5)

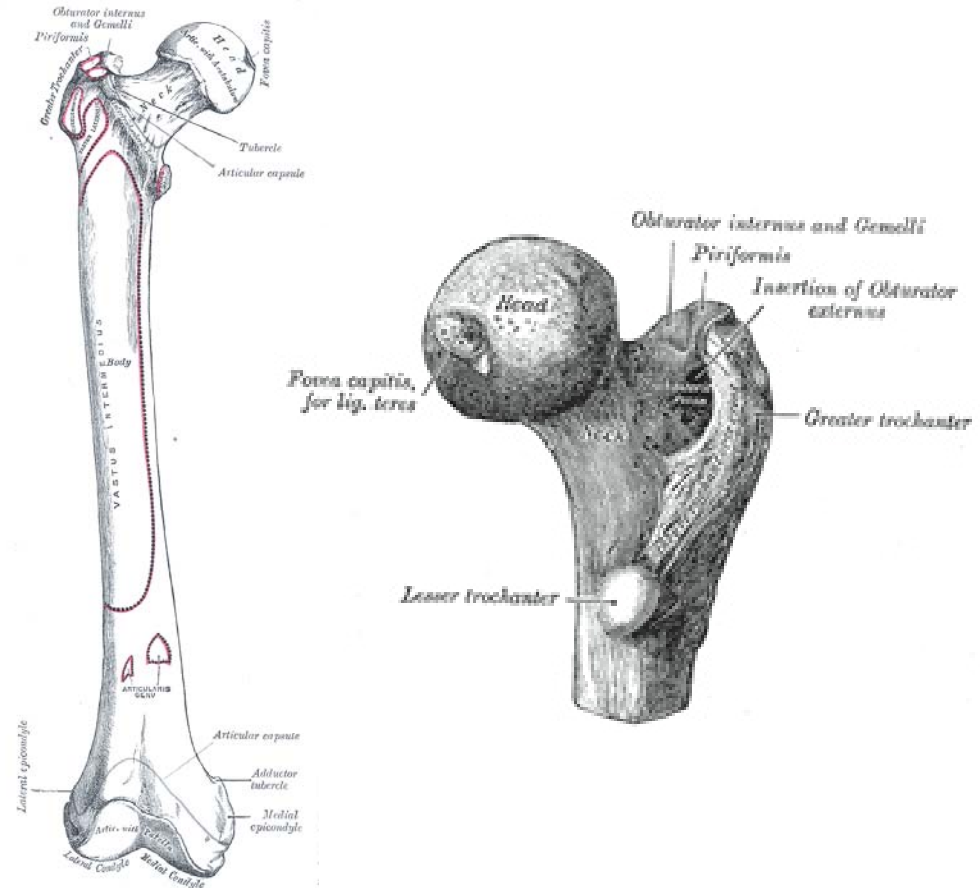


■ Bones

▣ Pelvis

- Hip bone (ilium, ischium and pubis)
- Coccyx
- Sacrum

▣ Femur



Henry Gray, 1918, *Anatomy of the human Body*

Hip Anatomy (2/5)

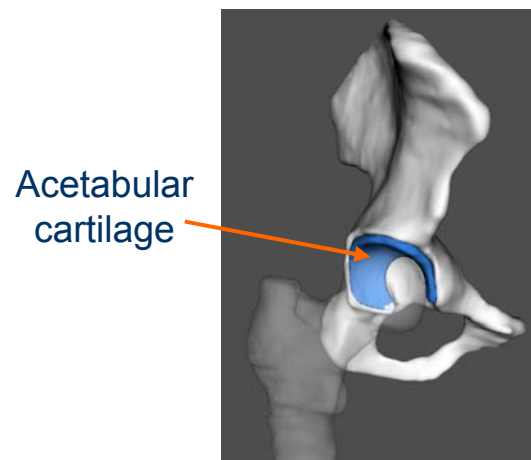
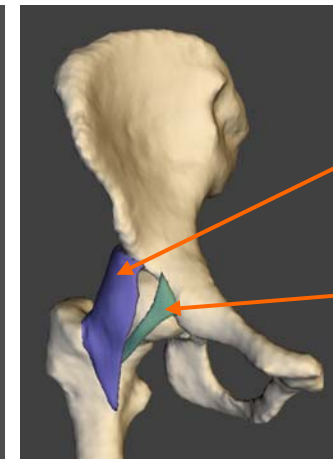
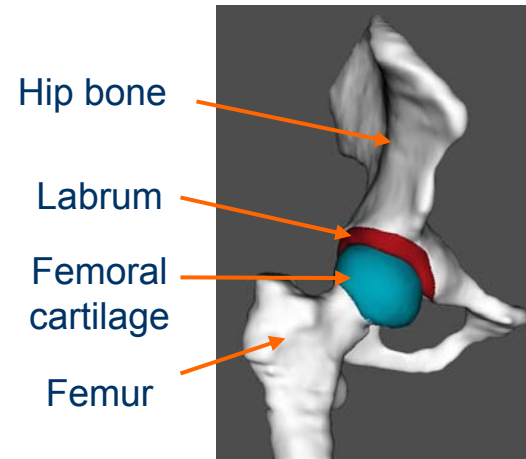


■ Cartilages

- Labrum
- Femoral
- Acetabular

■ Ligaments

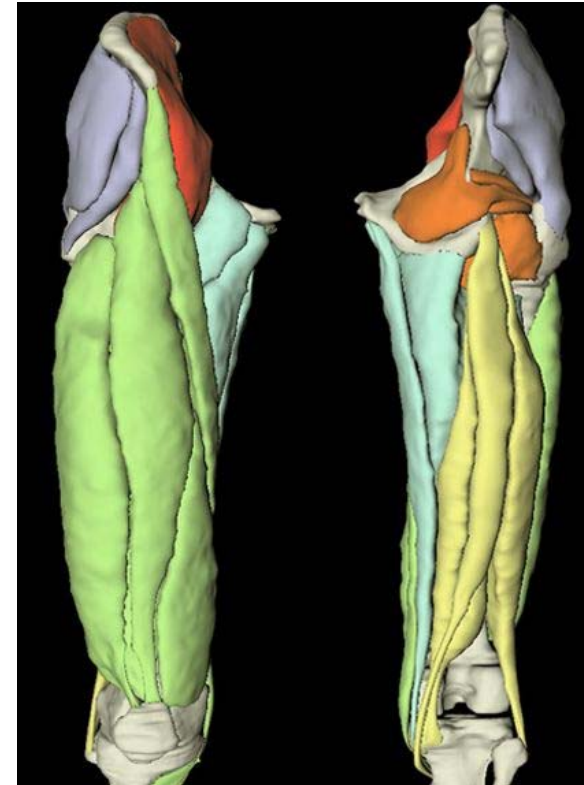
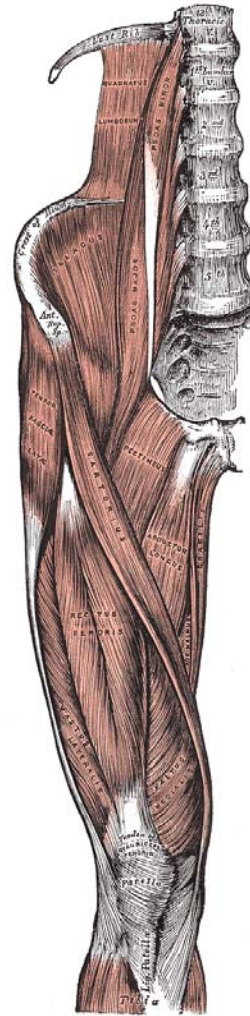
- Iliofemoral
- Pubofemoral
- Ischiofemoral



Hip Anatomy (3/5)



- Muscles of hip are those that cause movement in the hip
 - Muscles of iliac region
 - Muscles of thigh

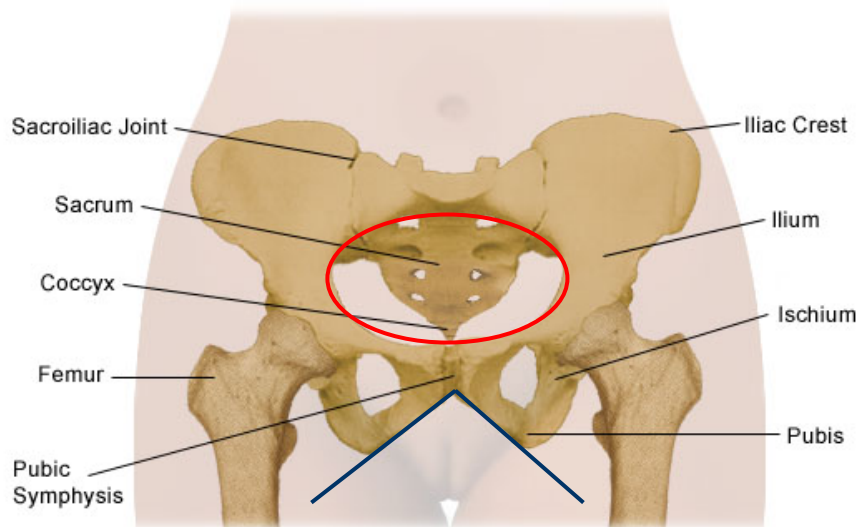


Hip Anatomy (4/5)

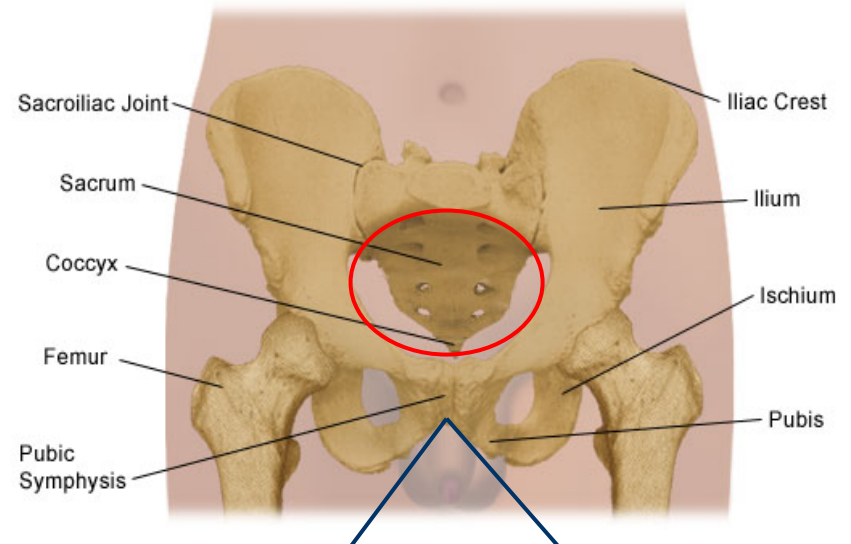


■ Female/ Male differences

Female Pelvis



Male Pelvis



Hip Anatomy: Joint (5/5)

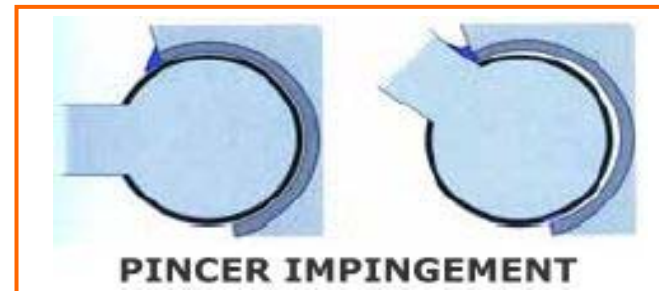
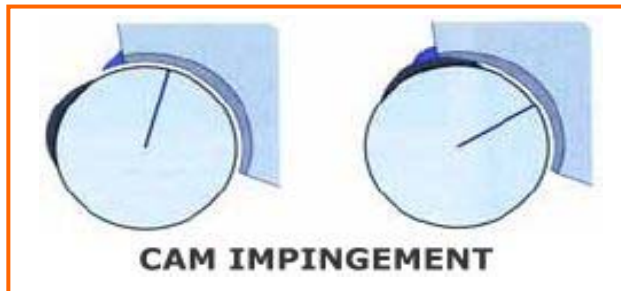


- Synovial joint
 - Wide range of movement (abduction/ adduction, flexion/ extension, int./ ext. rotation)
 - Capsule with lubricating fluid
- Modeled as a ball and socket joint
 - True for low amplitude movements
 - Not always valid with extreme movements (slight translations of rotation center)

Clinical Context



- Osteoarthritis (OA): hip joint degeneration
- Symptoms: impairment, stiffness, pain, inflammation and loss of mobility [1]
- Attack major joints and affect the majority of individuals over 50
- Origin hypothesis: repetitive and abnormal collisions (impingements)



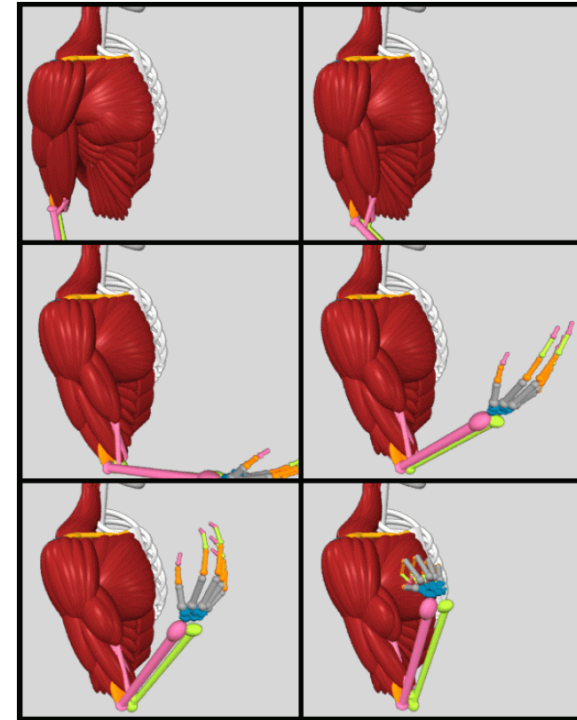
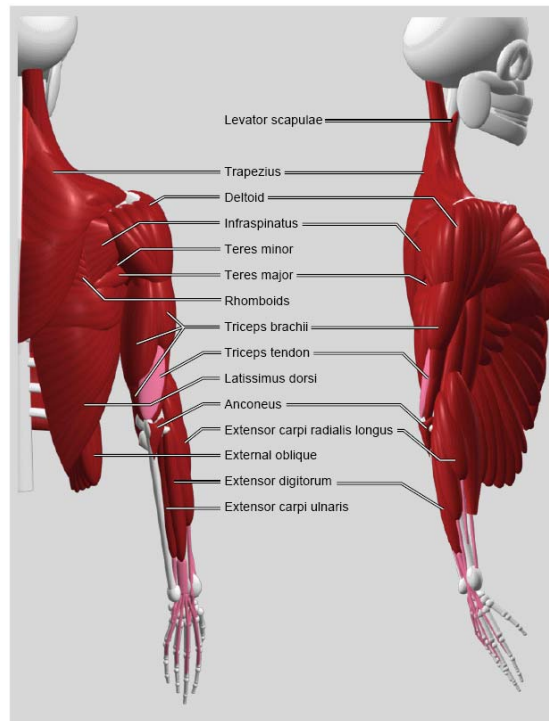
[1] D.T. Felson. *Clinical practice*. Osteoarthritis of the knee. N Engl J Med 354: 841-848, 2006

Musculoskeletal Modeling (1/4)



Scheepers et al. 97

- **Anatomical concepts**
 - **Anatomical constraints**
- BUT**
- **Not patient-specific**
 - **Unrealistic simplifications**



Scheepers, F.; Parent, R. E.; Carlson, W. E. & May, S. F. *Anatomy-based modeling of the human musculature*. SIGGRAPH '97, 1997, 163-172

Musculoskeletal Modeling (2/4)



Aubel and Thalmann 2001

- Anatomical Concepts (muscles, fat, bones)
- Anatomical constraints (e.g., attachments)

BUT

- Not patient-specific
- Interactive
- simplifications



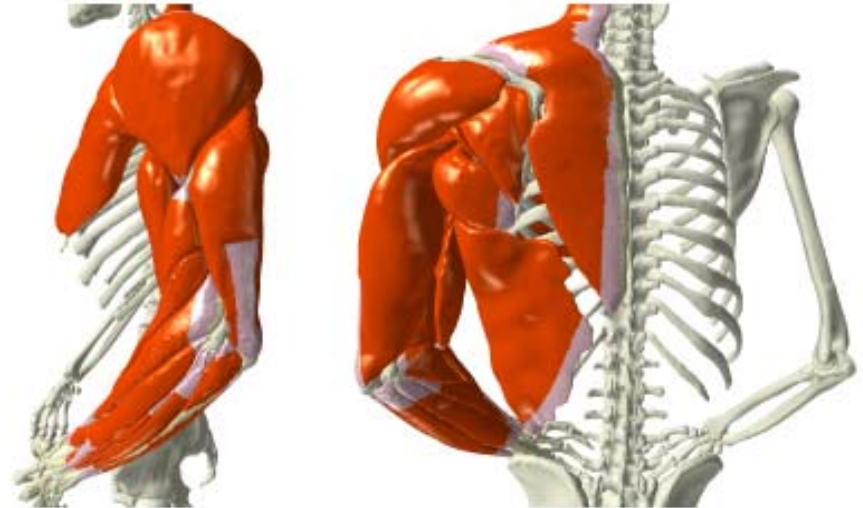
A. Aubel and D. Thalmann. *Interactive Modeling of the human musculature*. Computer Animation, 2001

Musculoskeletal Modeling (3/4)



Teran et al. 2005

- **Complex Anatomical Model (e.g., fiber direction, anisotropy, nonlinearity, FVM, fascia, etc.)**
 - **~Patient-specific (Visible Human Dataset)**
- BUT**
- **Interactive (e.g., manual correction and editing)**
 - **No medical validation**



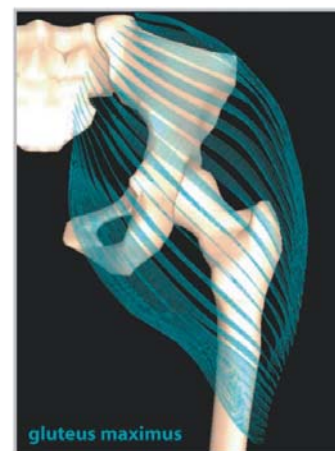
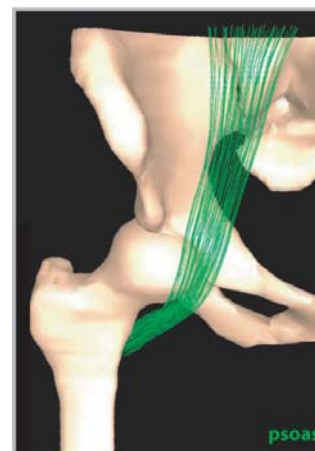
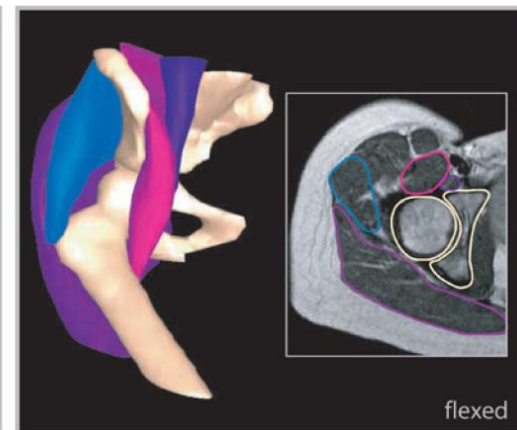
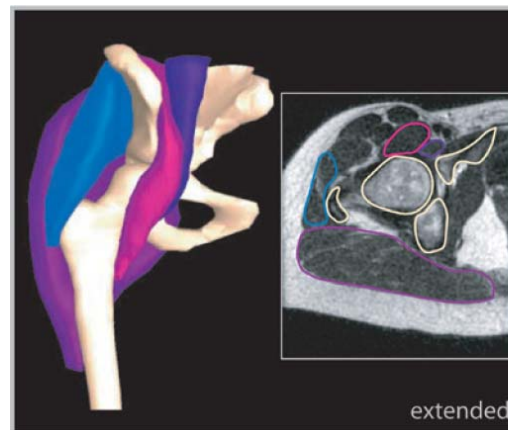
J. Teran, E. Sifakis, S.S Blemker, V. Ng-Thow-Hing, C. Lau and R. Fedkiw. *Creating and Simulating Skeletal Muscle from the Visible Human Data Set*. *IEEE Trans. Visual. Comput. Graph.*, 2005, 11, 317-328

Musculoskeletal Modeling (4/4)



Blemker and Delp 2005

- Complex Anatomical Model (e.g., fiber direction, FEM)
 - Patient-specific (MRI segmentation)
 - Medical validation
- BUT**
- Interactive (e.g., manual segmentation and attachments definition)



S. Blemker and S. Delp. *Three-Dimensional Representation of Complex Muscle Architectures and Geometries*. Annals of Biomedical Engineering, 2005, 33, 661-673

Hip Modeling (1/2)



- For what?
 - Improve understanding
 - Cause OA: repetitive femoro-acetabular impingement?
 - Improve detection
 - Support early diagnosis
 - Provide more automatic and objective assessment
 - Improve treatment
 - Support corrective surgery planning: bone and labrum resection
 - Support arthroscopy
- How?
 - Acquire
 - Choose an adequate modality and define a protocol
 - Segment
 - Devise an efficient segmentation approach that considers anatomical constraints
 - Analyze
 - Provide tools for data examination and diagnosis

- Requirements
 - High accuracy
 - Reasonable time
 - Acquisition + transfer time
 - Modeling time
 - Integration in clinical sites if possible
 - Direct clinical benefits
 - Provide valuable feedback
 - **Patient specific**

Modeling Problematic

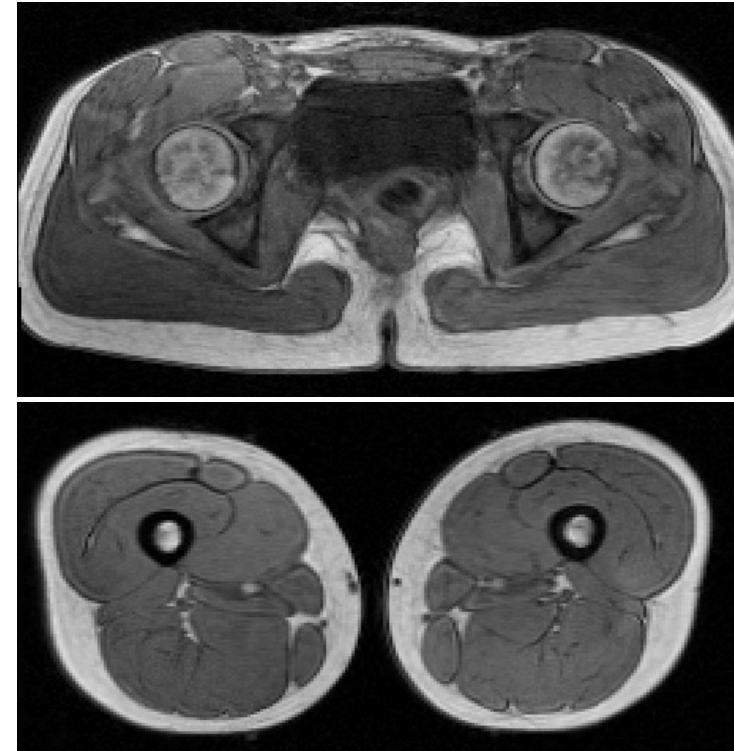


Goal: Extract from (multimodal) data patient anatomical structures

Context:

- **MRI**
 - Noise
 - A lot of textural information
 - Low resolution, partial volumes
- **Musculoskeletal system**
 - Many interconnected components in contact
 - Large displacements

- Requirements
 - Volumetric data
 - Non invasive
 - Routinely used
 - Soft and bony tissue
 - Versatile



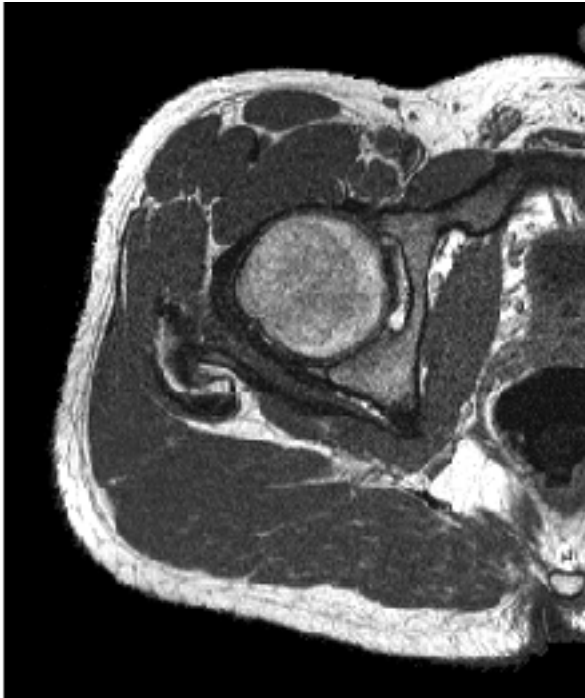
>> Magnetic Resonance Imaging (MRI)

Acquisition: MRI (2/9)

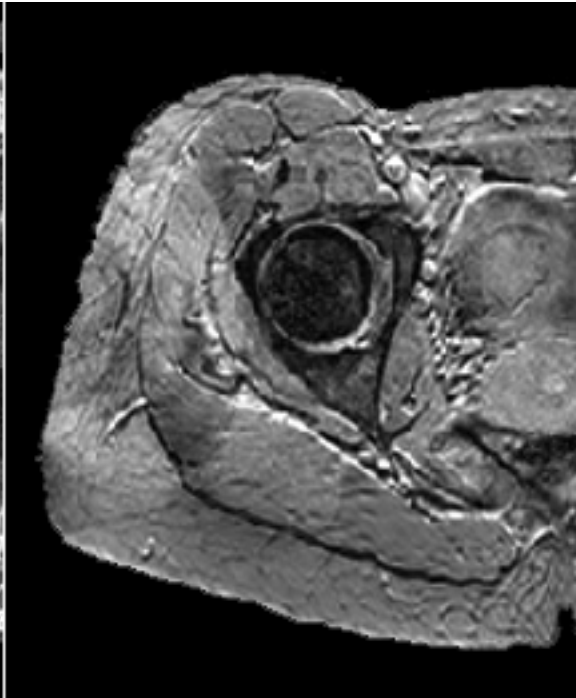


- MRI aims at measuring the signal from the resonance of hydrogen atoms, contained in all tissues (water)
- In particular, MRI considers
 - T1 (longitudinal) and T2 (transversal) relaxation times
 - Proton density (tissue concentration in water)
 - Fluid flow

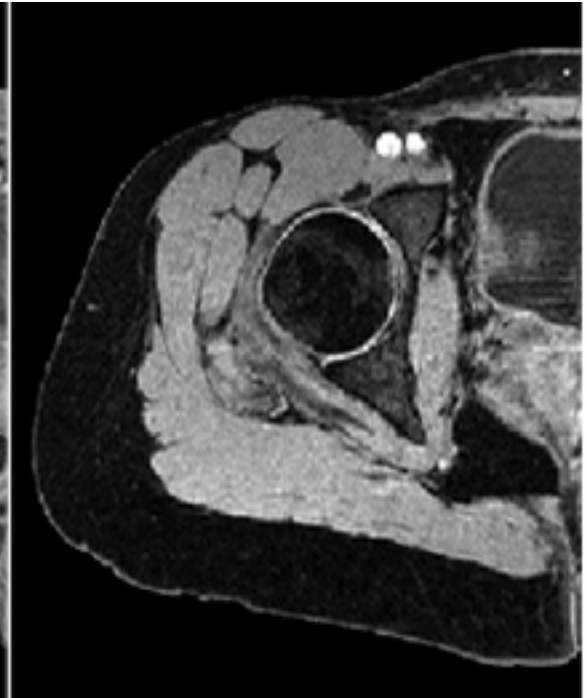
Acquisition: MRI (3/9)



Spin-echo T1,
TR=578ms, TE=18ms



Gradient-echo T2*,
TR=30ms, TE=14ms



Gradient-echo T1,
TR=20ms, TE=7ms

Acquisition: MRI (4/9)



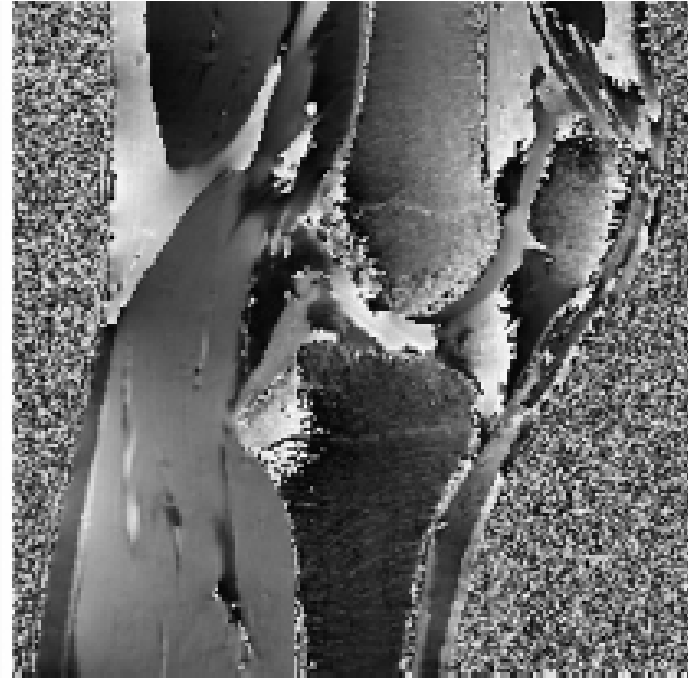
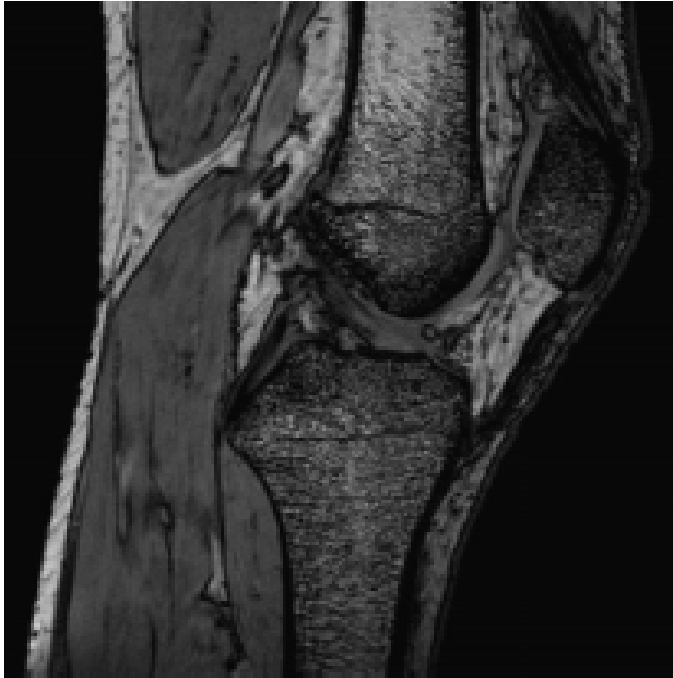
T1-Weighted Short TR =
bone highlight

Fat suppressed scan

Difference image
(more adapted
for segmentation)

R. Dalvi, R. Abugharbieh, D. C. Wilson and D. R. Wilson. *Multi-Contrast MR for Enhanced Bone Imaging and Segmentation*. International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC), Lyon-France, 2007, 5620-5623

Acquisition: MRI (5/9)

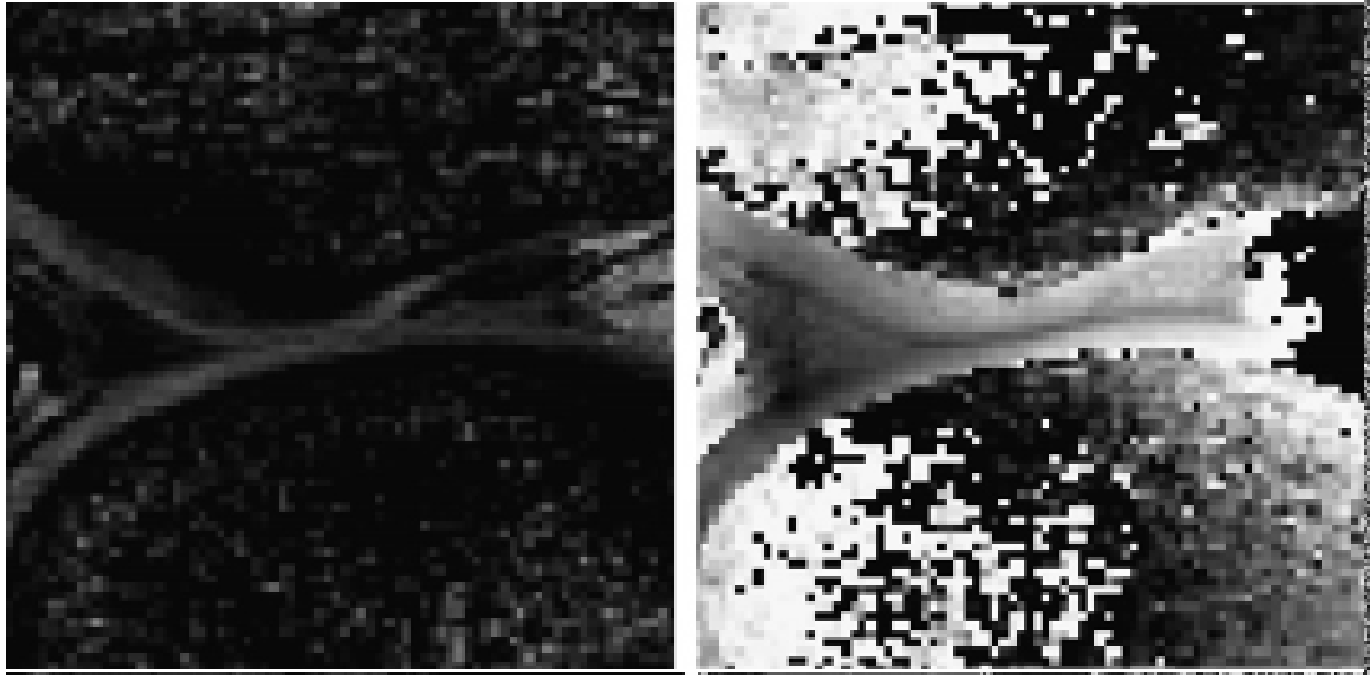


Magnitude of complex MRI signal

Phase of complex MRI signal

P. Bourgeat, J. Fripp, P. Stanwell, S. Ramadan and S. Ourselin. *MR image segmentation of the knee bone using phase information*. Medical Image Analysis, 2007, 11, 325-335

Acquisition: MRI (5/9)



Detail: knee cartilage

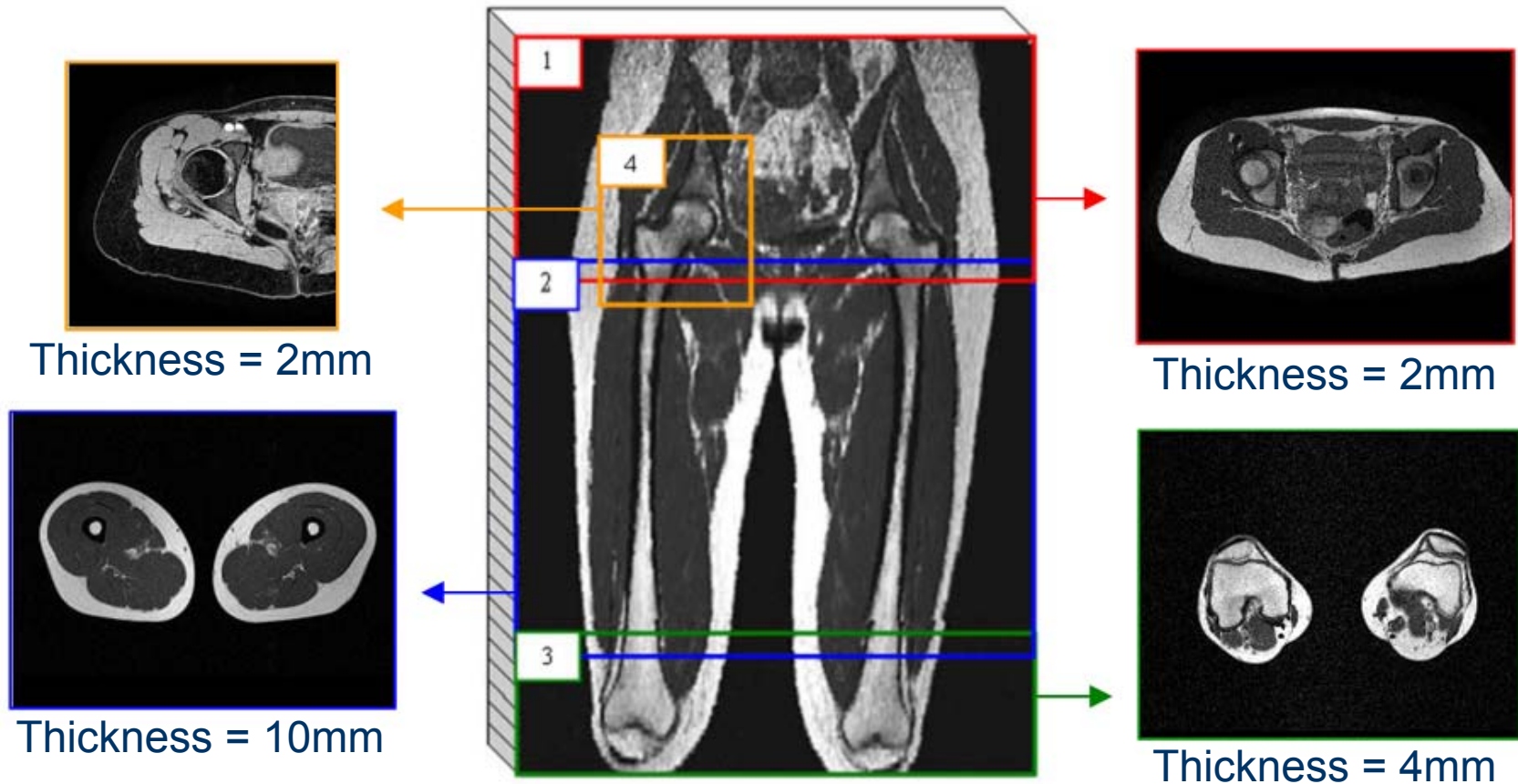
Magnitude of complex MRI signal

Phase of complex MRI signal

P. Bourgeat, J. Fripp, P. Stanwell, S. Ramadan and S. Ourselin. *MR image segmentation of the knee bone using phase information*. Medical Image Analysis, 2007, 11, 325-335

Acquisition: MRI (6/9)

MIRALab - HUG

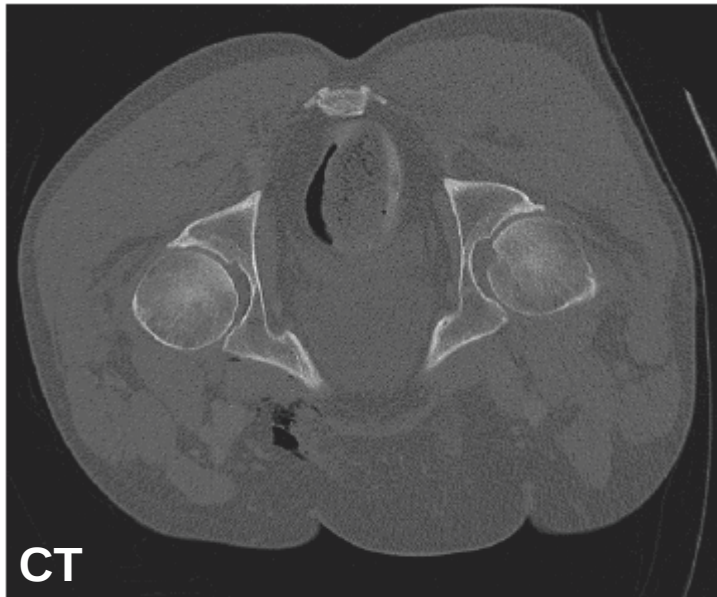


#1,2,3: Axial 2D T1 Turbo Spin Echo (TSE), TR/TE= 578/18 ms, resolution=0.78x0.78mm

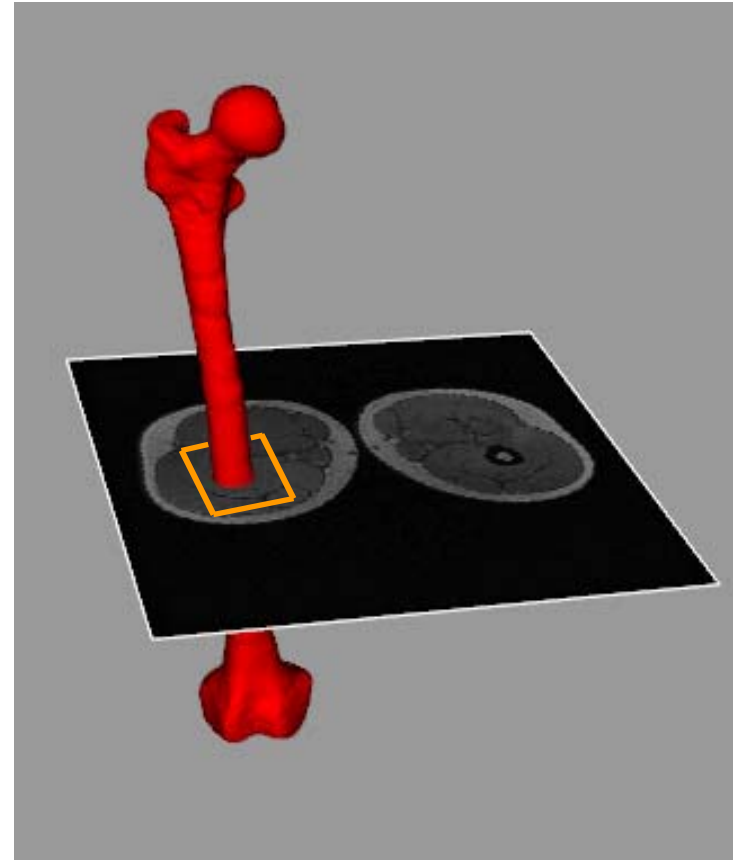
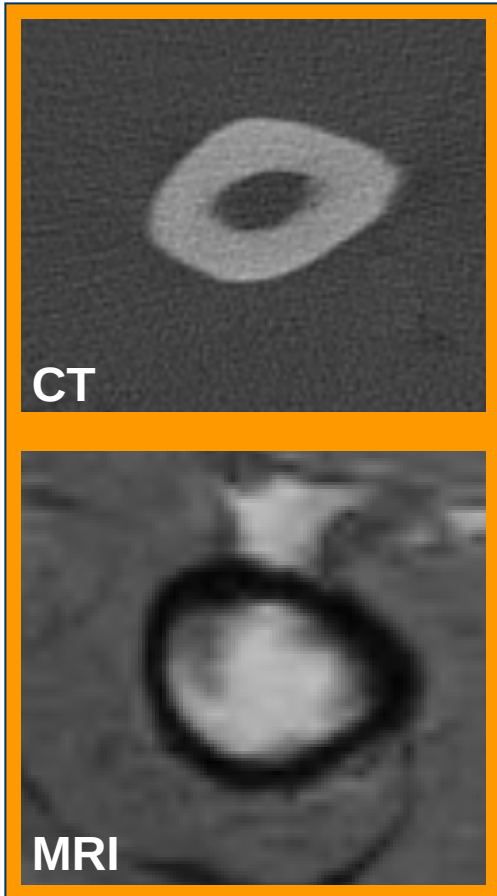
#4: Axial 3D T1 Gradient Echo, TR/TE= 20/7 ms, resolution=0.78x0.78mm

- Computed Tomography (CT)
 - Appropriate for bone imaging but some difficulties in presence of osteoporosis
 - Visualization of soft tissues is difficult
 - Invasive (exposure to X-ray radiation)

Acquisition: CT vs MRI (8/9)



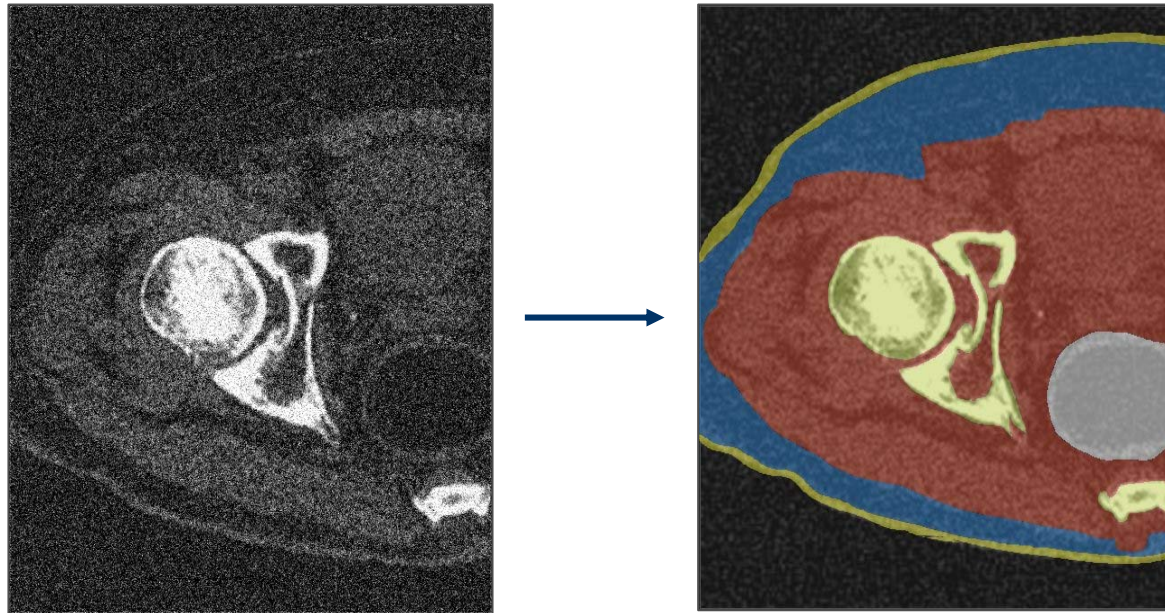
Acquisition: CT vs MRI (9/9)



Segmentation: definition



- Image partitioning
 - non overlapping regions
 - homogeneous regions



Segmentation: requirements



- **Flexibility**
 - Fit different type of organs (i.e., soft and bony organs)
- **Control**
 - Regularization
 - Constraints consideration
 - Possible interaction
- **Efficiency**
 - Robust to image noise and artefacts
 - Fast computation
 - Multi-resolution
- **Accuracy**

Segmentation: categories



- Direct segmentation methods
 - Thresholding
 - Region growing
 - Edge detection
 - Classification
- Registration methods
 - Image to image
 - Model to image
 - Model to model
- Hybrid methods

Direct Segmentation (1/2)



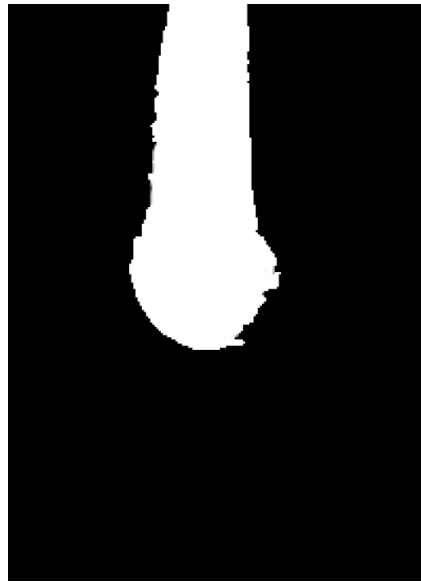
For complex problems, direct segmentation is:

- Noise-sensitive
- Not robust
- Quite inaccurate

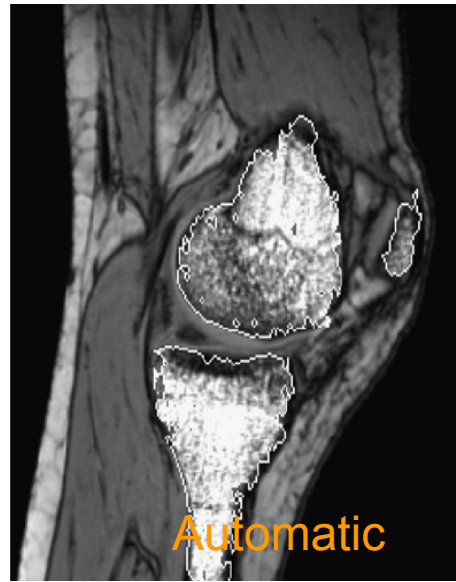
Direct Segmentation (2/2)



As a result, additional and more complex stages are used for a more efficient direct segmentation (e.g., training, pre-processing)



Dalvi et al.: MRI protocol
+ region growing



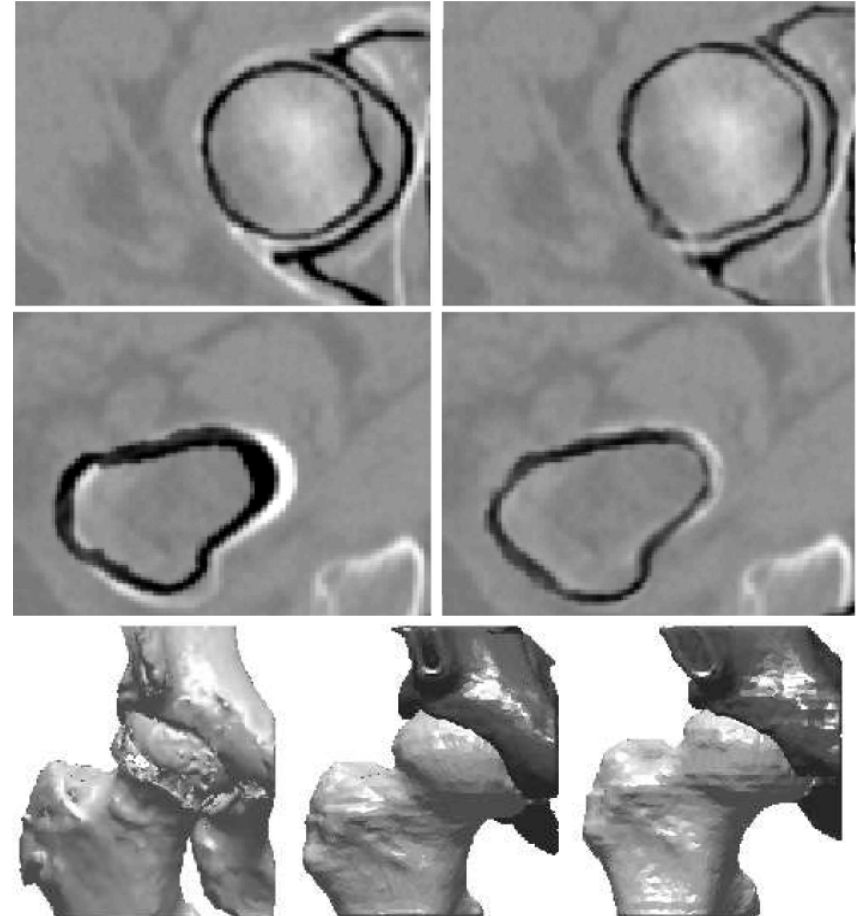
Bourgeat et al.: MRI protocol +
classification (SVM)

Image to Image registration



Pettersson et al. 2006

- Quadrature phase registration
- Multiscale and regularization
- Shape constraints not present
- Time?



J. Pettersson, H. Knutsson and M. Borga. *Automatic Hip Bone Segmentation Using Non-rigid Registration*. ICPR, 2006, 3, 946-949

Model to Image registration

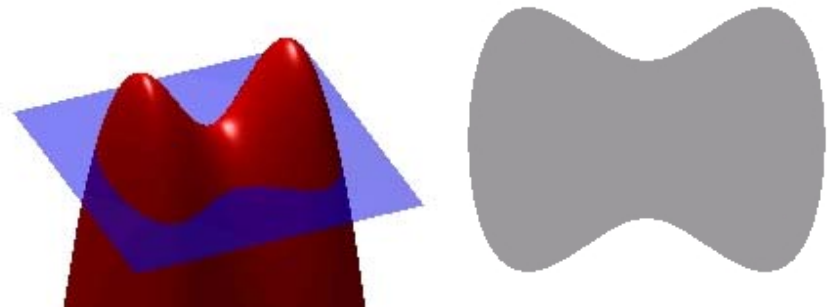


Lorigo et al. 1997

- Geodesic Active Contours
- Level set
- Exploit intensity and variance
- Cortical/ trabecular Intensity problem
- Possible leaking

$$E[(C)(p)] = \int_0^1 \underbrace{g(|\nabla I(C(p))|)}_{\text{Boundary attraction}} \underbrace{|\dot{C}(p)|}_{\text{Regularity}} dp$$

$$C_t = [g(|\nabla I|)\mathcal{K} - \nabla g(|\nabla I|) \cdot \mathcal{N}]\mathcal{N}$$



$$\phi_t = g(|\nabla I|)\mathcal{K}|\nabla \phi| + \nabla g(|\nabla I|) \cdot \nabla \phi$$

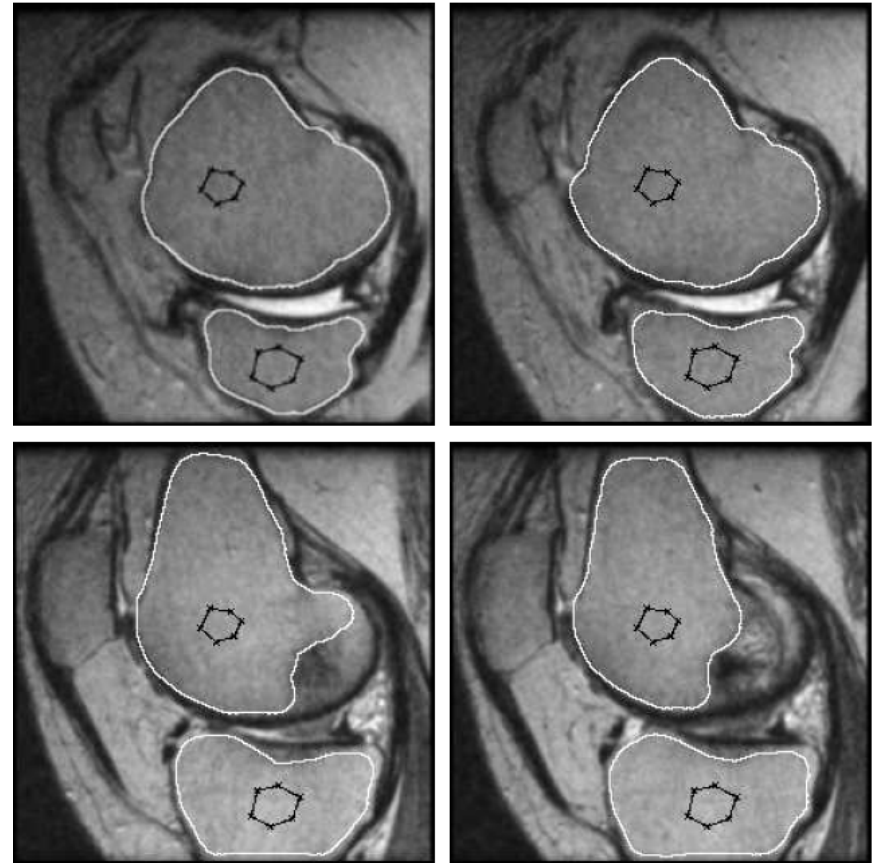
L. M. Lorigo, O.D. Faugeras, W.E.L. Grimson, R. Keriven and R. Kikinis. *Segmentation of Bone in Clinical Knee MRI Using Texture-Based Geodesic Active Contours*. MICCAI, 1998, 1195-1204

Model to Image registration



Lorigo et al. 1997

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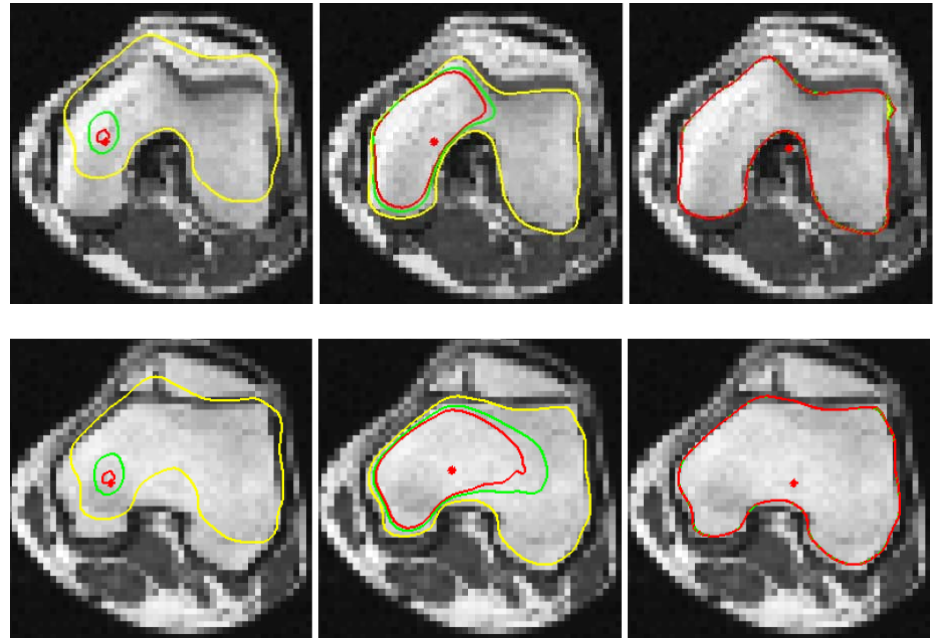
L. M. Lorigo, O.D. Faugeras, W.E.L. Grimson, R. Keriven and R. Kikinis. *Segmentation of Bone in Clinical Knee MRI Using Texture-Based Geodesic Active Contours*. MICCAI, 1998, 1195-1204

Model to Image registration



Leventon et al. 2000

- Levelset evolution
- PCA regularization
- MAP formulation
- Difficult to consider constraints
- Potential cortical/trabecular Intensity problem



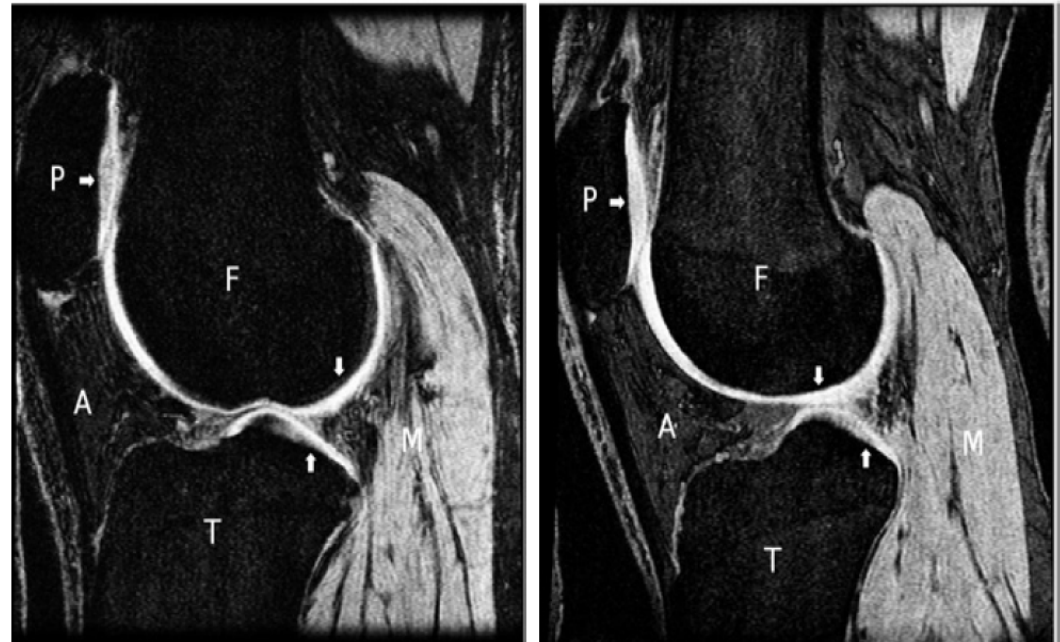
M.E. Leventon, W.E.L. Grimson and O. Faugeras. *Statistical shape influence in geodesic active contours*. CVPR, 2000, 1, 316-323

Model to Image registration



Fripp et al. 2004

- SSM
- Fat suppressed MRI

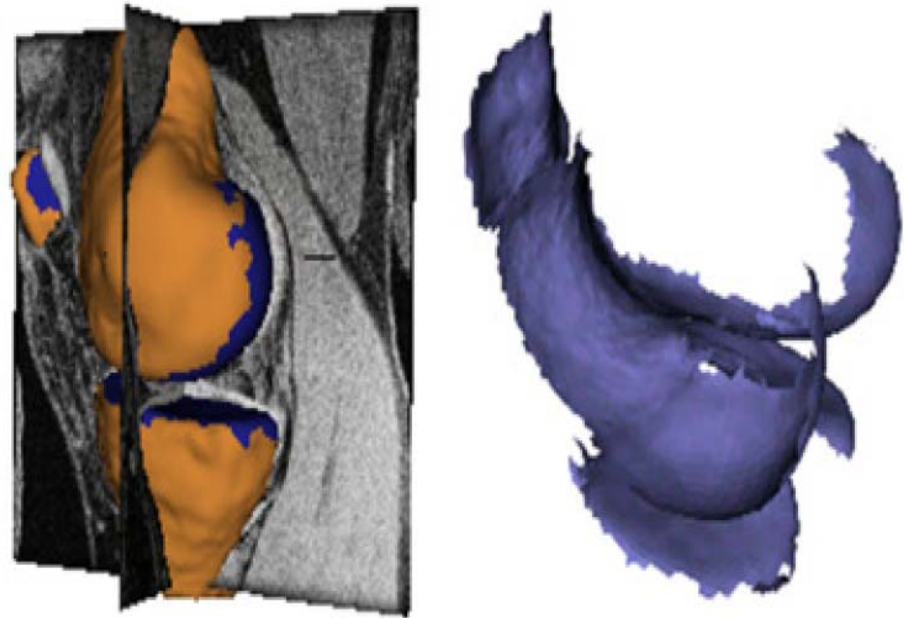


Model to Image registration



Fripp et al. 2004

- SSM
- Fat suppressed MRI
- Gradient as clue
- Cartilage extraction

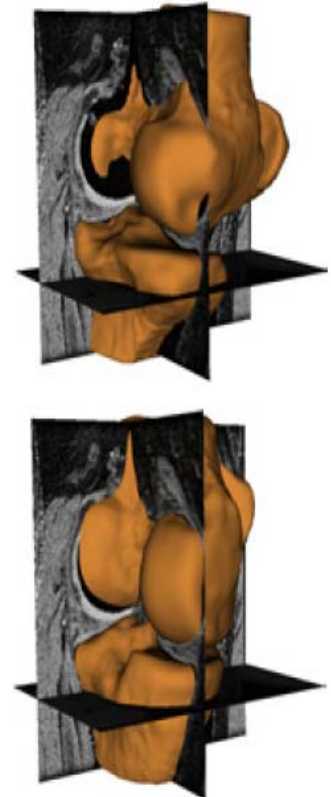
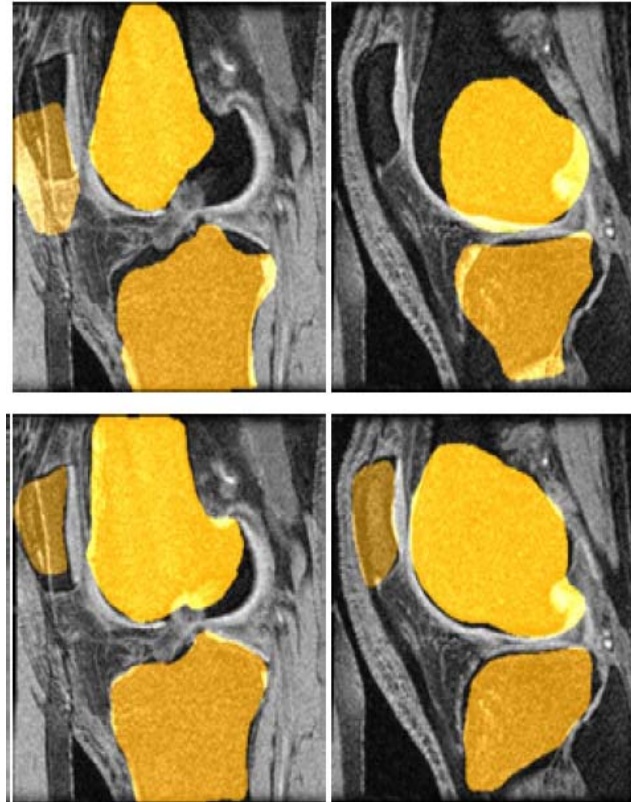


Model to Image registration

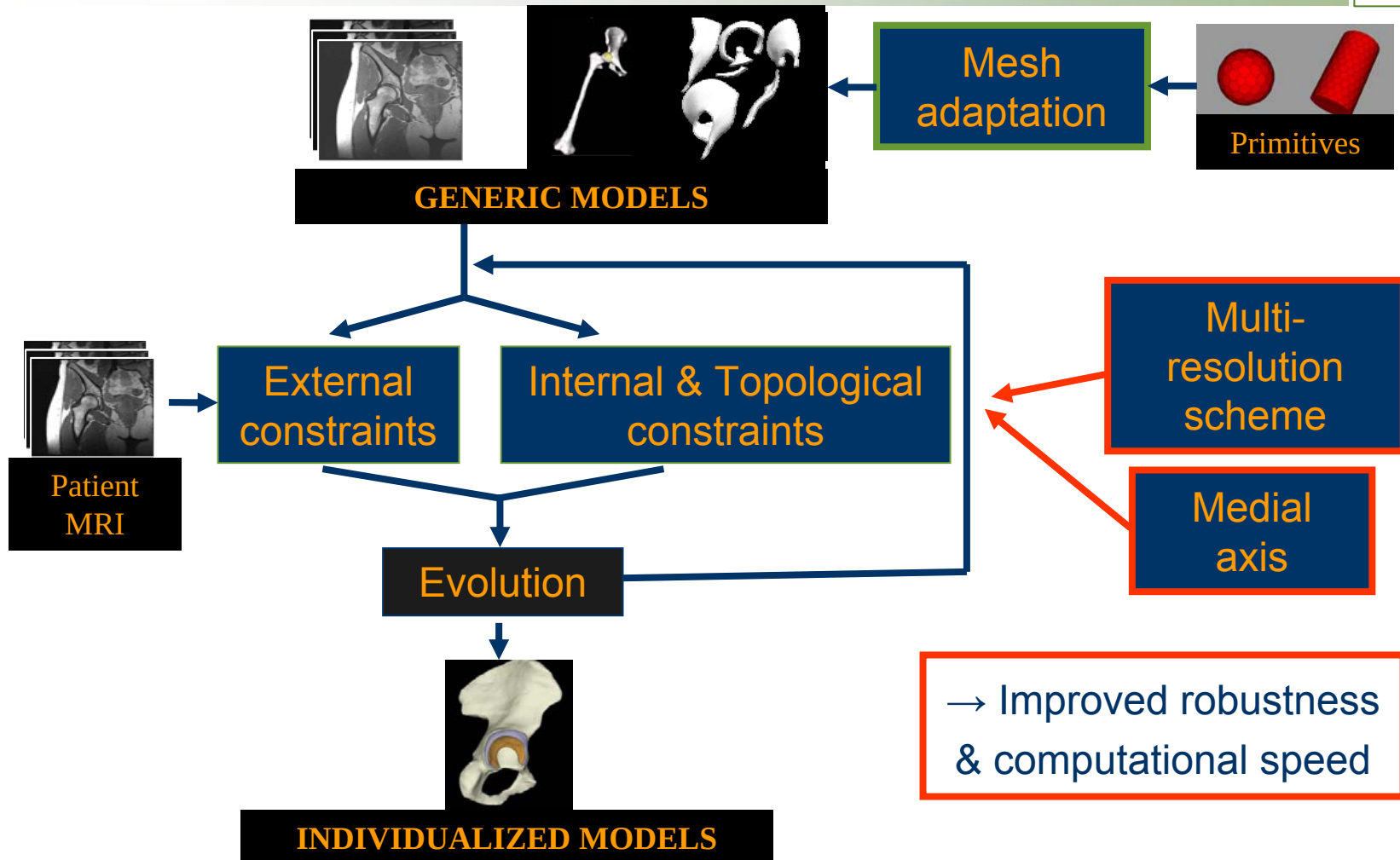


Fripp et al. 2004

- SSM
- Fat suppressed MRI
- Gradient as clue
- Cartilage extraction
- Errors



Proposed Segmentation

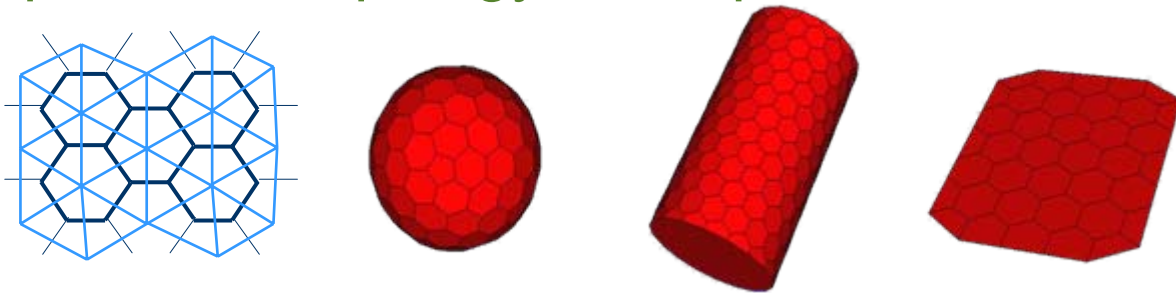


B. Gilles, *Anatomical and kinematical modelling of the musculoskeletal system from MRI*.
Ph.D. dissertation, Université de Genève, 2007.

Generic Model Creation (1/3)



- 2-Simplex meshes [1][2]
 - Dual to triangle mesh
 - Each vertex has exactly 3 neighbors
 - Simple local geometric description (3 similitude-invariant “simplex parameters”)
 - Simple mesh topology description



[1] Delingette, H. *General Object Reconstruction Based on Simplex Meshes*. Int. J. Comput. Vis., 1999, 32, 111-146

[2] J. Montagnat and H. Delingette. *4D deformable models with temporal constraints: application to 4D cardiac image segmentation*. Medical Image Analysis, 9(1), 87-100, 2005

Generic Model Creation (2/3)

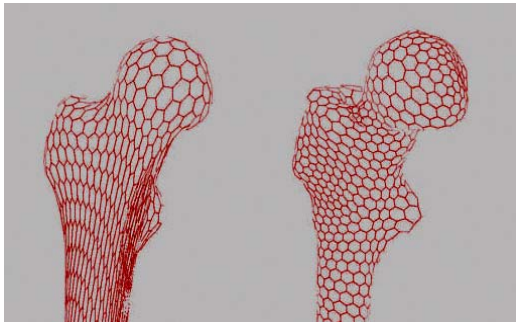


- Coarse construction

- from a series of constraints (points manually defined in MRI) primitives are deformed to match the structures of interest

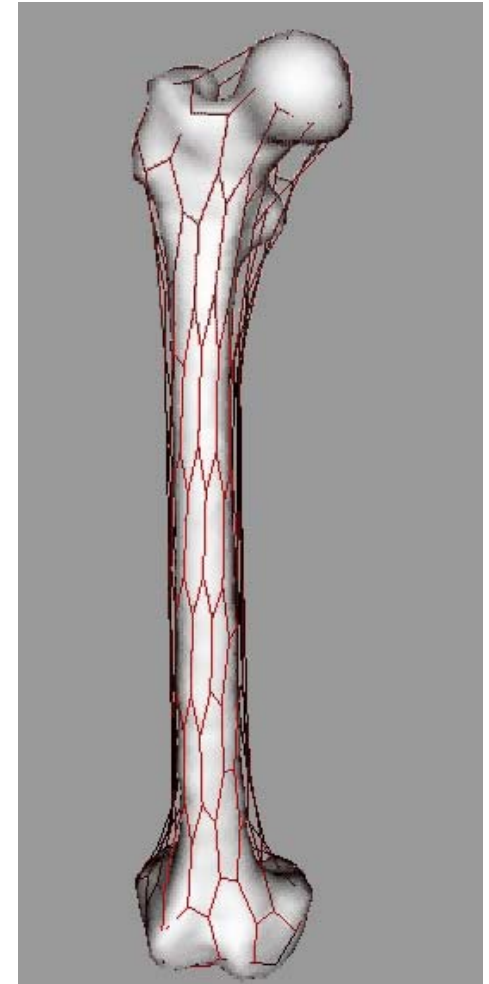
- Refinement:

- Topological optimization to get a quasi regular triangulation



Without topology
optimization

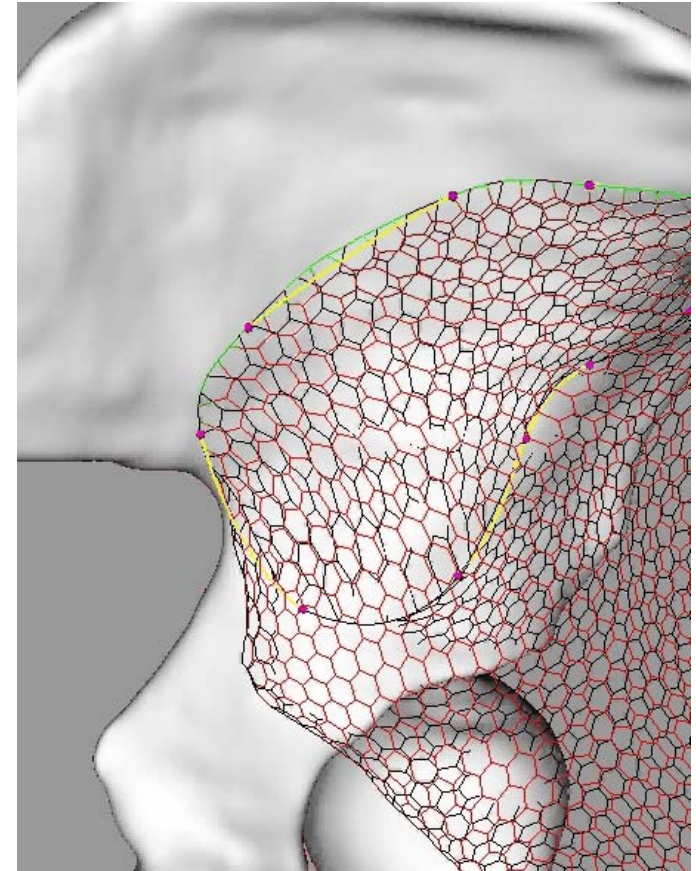
With topology
optimization



Generic Model Creation (3/3)



- Bone/ Muscle attachment
 - Splines parameterization
 - 50 generic attachments
 - Rely on anatomical assumptions [1]
- Cartilage/ Bone attachment
- Muscle/ Muscle contact
 - Fascia modeling



[1] B.L. Kaptein and F.C,T Van Der Helm. *Estimating muscle attachment contours by transforming geometrical bone models*. J. Biomech, 37, 263-273, 2004.

- lumped mass particles submitted to forces
- Newtonian law of motion
 - Euler implicit

$$\begin{cases} \mathbf{P}_{t+dt} - \mathbf{P}_t &= (\mathbf{V}_t + (\mathbf{V}_{t+dt} - \mathbf{V}_t))dt \\ \mathbf{V}_{t+dt} - \mathbf{V}_t &= \mathbf{H}^{-1}\mathbf{Y} \end{cases}$$

where

$$\begin{cases} \mathbf{H} &= \mathbf{I} - \mathbf{M}^{-1} \frac{\partial \mathbf{F}}{\partial \mathbf{V}} dt - \mathbf{M}^{-1} \frac{\partial \mathbf{F}}{\partial \mathbf{P}} dt^2 \\ \mathbf{Y} &= \mathbf{M}^{-1} \mathbf{F}(\mathbf{P}_t, \mathbf{V}_t) dt + \mathbf{M}^{-1} \frac{\partial \mathbf{F}}{\partial \mathbf{P}} \mathbf{V}_t dt^2 \end{cases}$$

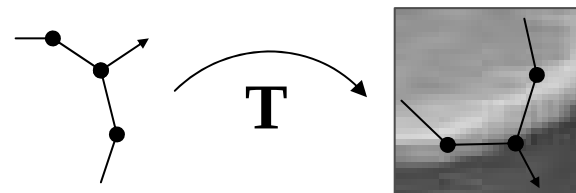
External Forces (1/2)



■ Image forces

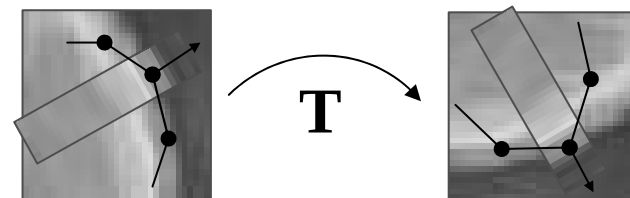
- Align model with model contours in image

- Maximize gradient magnitude
- Align model and image gradient



- Register reference with image features

- Intensity profiles matching
- Similarity measure



External Forces (2/2)



■ Collision

▫ Collision detection

- Deformable/ deformable: bounding box hierarchy
- Rigid/ Deformable: distance maps

▫ Collision response [1]

- Penalty forces
- Velocity/ position alteration

■ Constraints

▫ Attachments

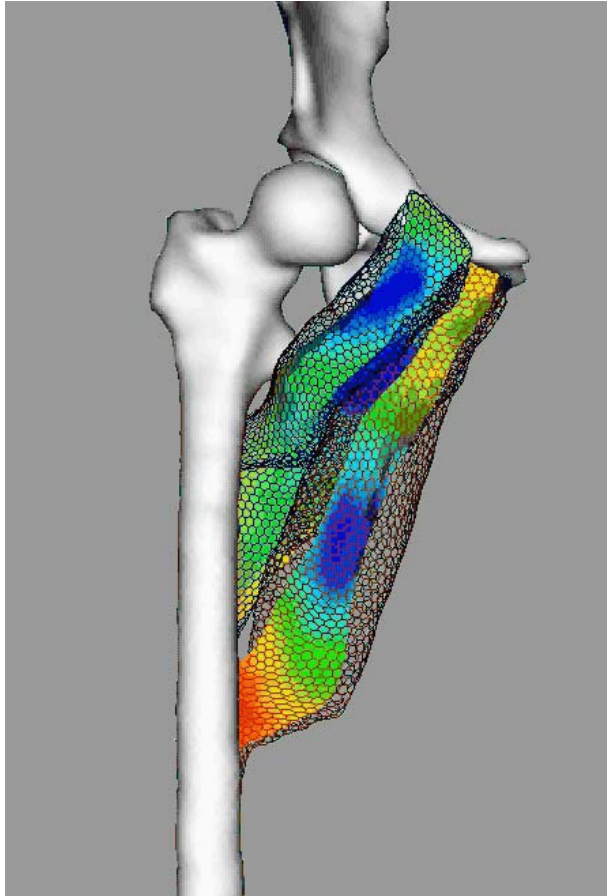
- Mass modification [2]

▫ Contact

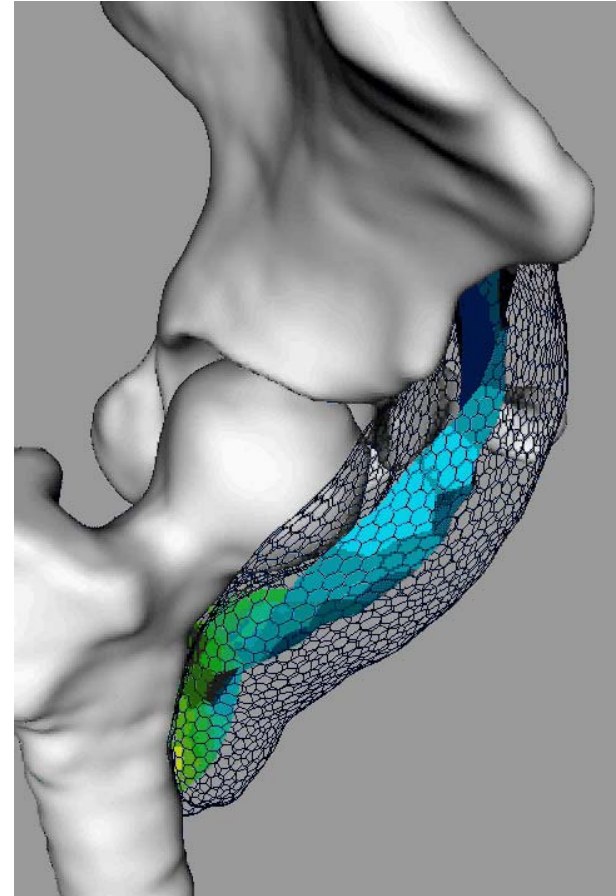
[1] P. Volino and N. Magnenat-Thalmann. *Implementing fast Cloth Simulation with Collision Response*. Comput. Graph. Int., 257-266, 2000.

[2] D. Baraff and A. Witkin. *Large Steps in Cloth Simulation*. SIGGRAPH'98, 43—54, 1998

External Forces (2/2)



Deformable/ deformable

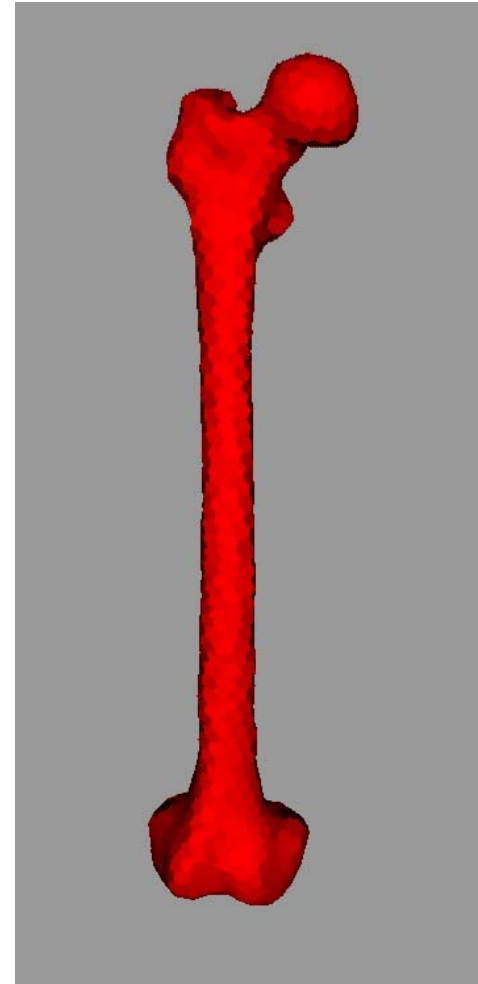


Rigid/ deformable

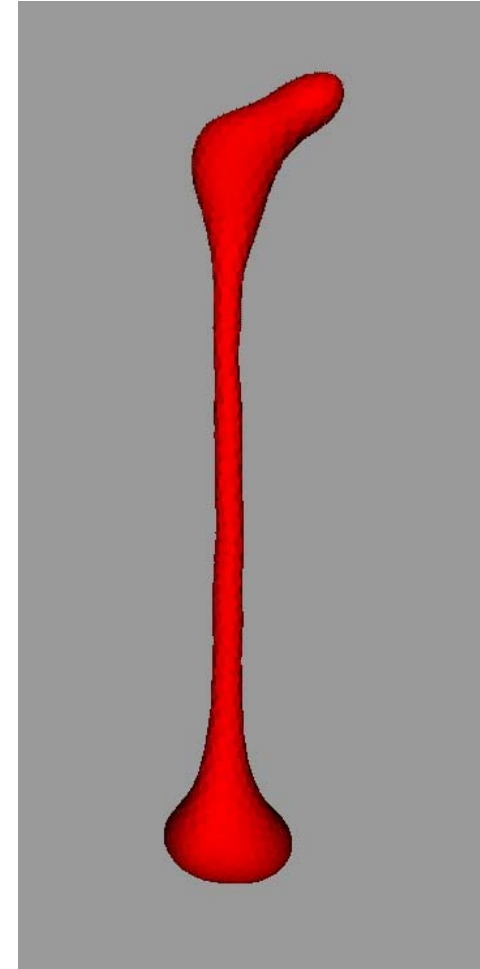
Internal Forces (1/3)



- Smoothing forces
 - Laplacian smoothing
 - Shrink effect
 - Bending force (curvature average)
 - Modify tangential term
 - Consider 2nd order neighbor

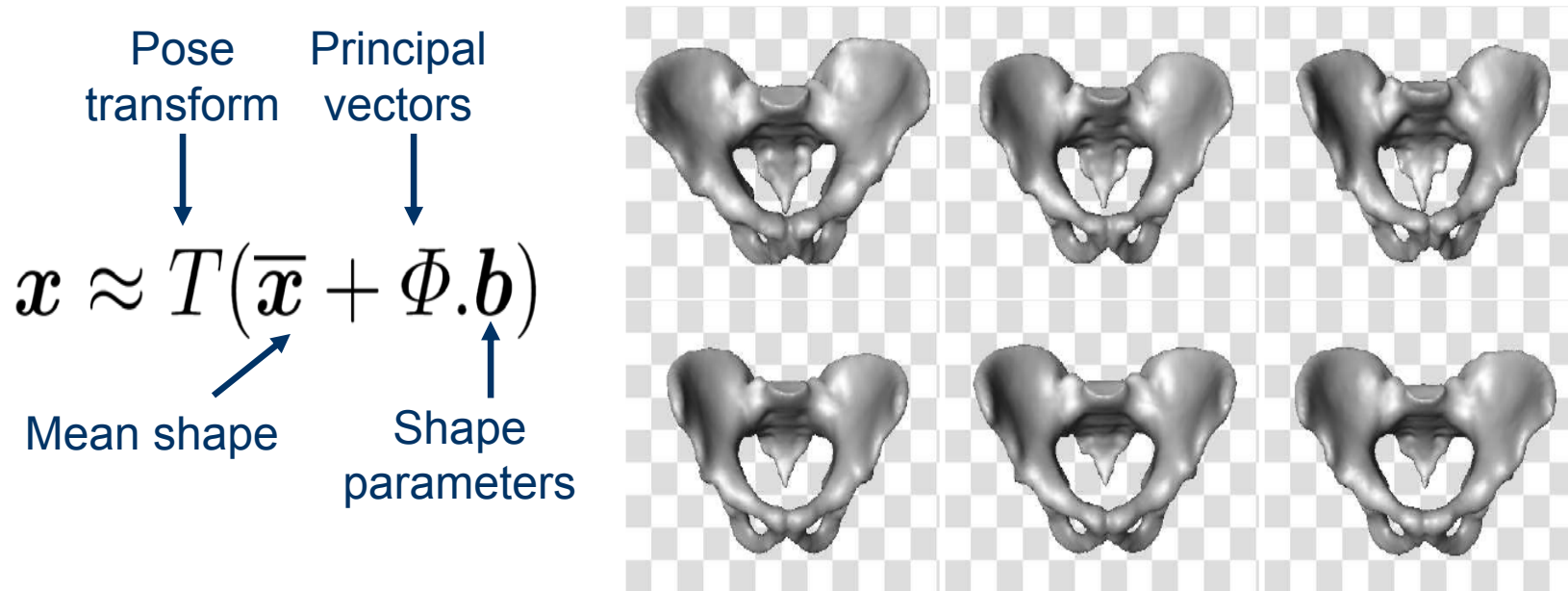


- Shape forces
 - Strain energy
 - Matching to a reference local geometry
 - Use of reference simplex parameters



- Shape forces

- Principal Component Analysis (PCA)



Reproduced from [1]

[1] H. Lamecker, M. Seebass, H-C Hege, P. Deuflhard. *A 3D statistical Shape Model Of The Pelvic Bone For Segmentation*. SPIE, 2004.

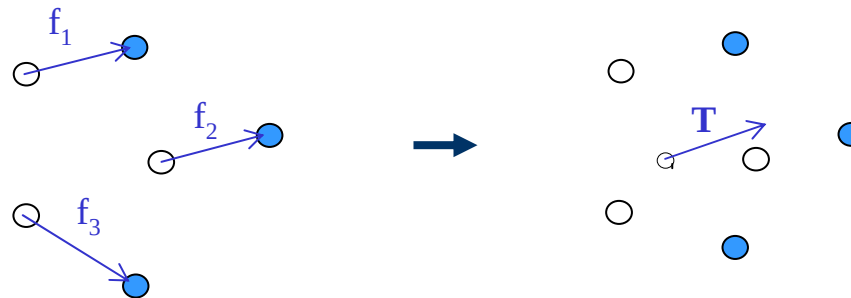
- Shape forces
 - PCA regularization
 - Discard “invalid” shapes
 - Exploit LODs and alignment transform type [1]
 - Correspondence problem
 - Training dataset
 - Linearity/ sufficient statistics

[1] J. Schmid and N. Magnenat-Thalmann. *MRI Bone Segmentation using Deformable Models and Shape Priors*. MICCAI 2008.

Forces regularization



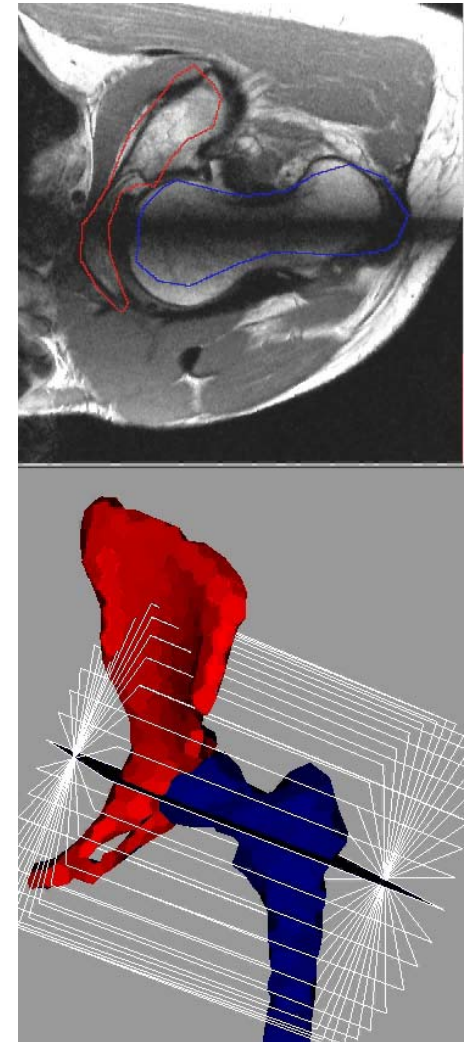
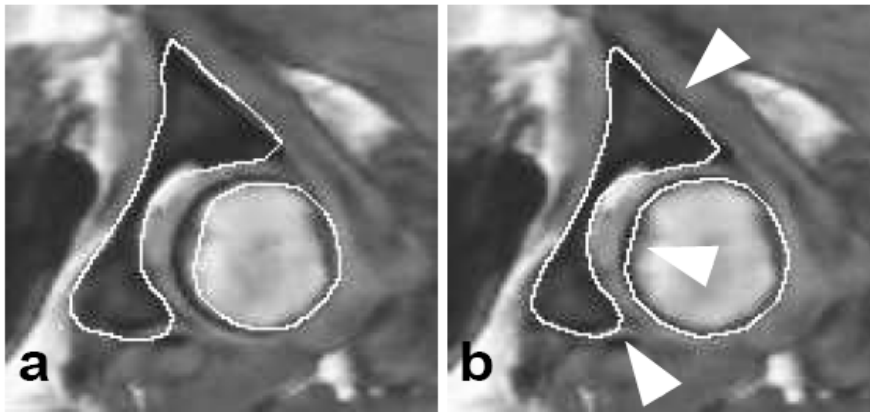
- Locally, noise and adjacent structures can affect the external forces computation
- Use “pair & smooth” approach to find a global transformation T from local displacements f_i



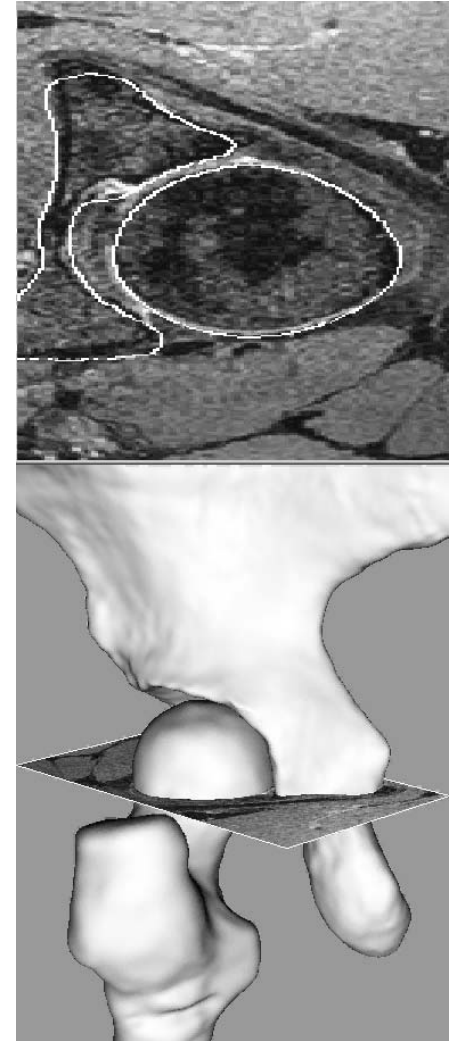
- Progressively decrease the regularization influence

Results (1/4)

- Bone Modeling
 - Comp. time ~2min
 - accuracy ~1.5mm
 - Validated on low resolution images



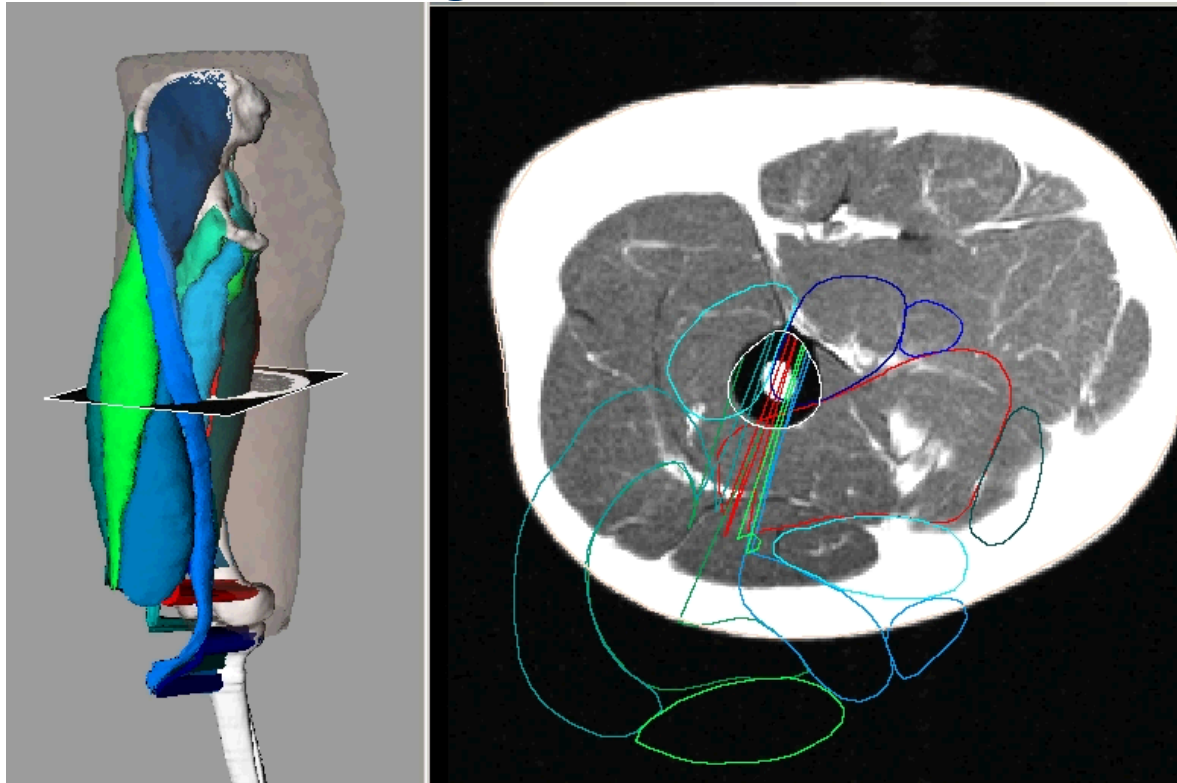
- Periarticular tissue modeling
 - 3 cartilages and 3 ligaments
 - Automatic initialization from bones
 - Computation time ~3min
 - Mostly relies on geometric constraints
 - Shape and smoothness
 - Contacts
 - Thickness
 - Validation difficult



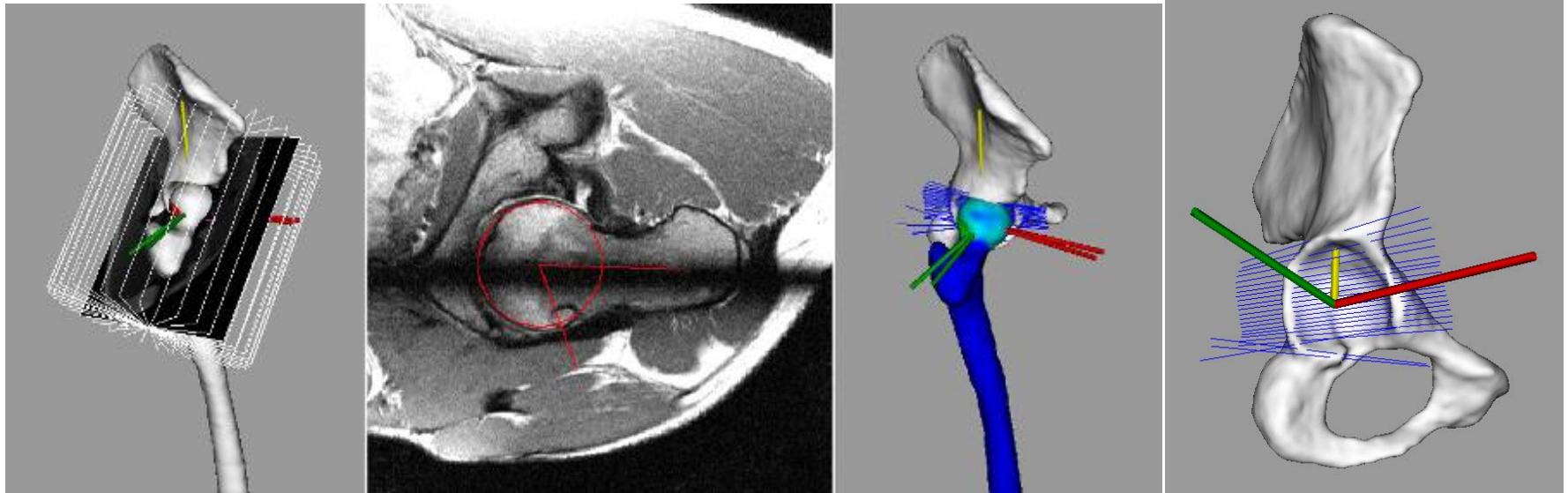
- Muscle Modeling
 - 21 muscles in contact
 - Automatic initialization from bones
 - Comp. time ~10min
 - accuracy ~1.5mm

Results (3/4)

- Muscle Modeling



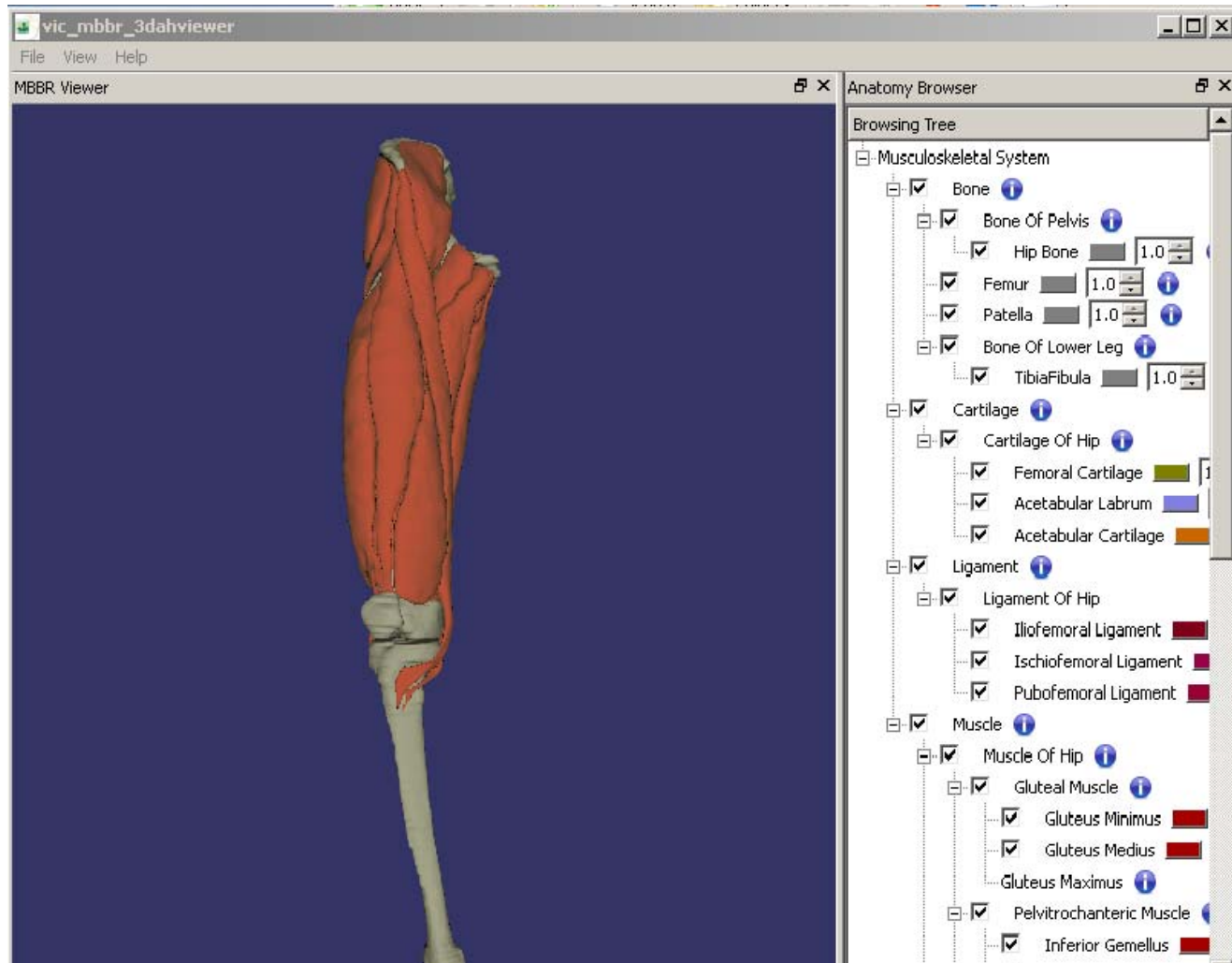
■ Analysis



[1] C.W.A. Pfirrmann, B. Mengiardi, C. Dora, F. Kalberer, M. Zanetti and J. Hodler. *Cam and Pincer Femoroacetabular Impingement: Characteristic MR Arthrographic Findings in 50 Patients*. Radiology, 240(3), 778-785, 2006.

[2] D. Reynolds, J. Lucas and K. Klaue. *Retroversion of the acetabulum: A cause of hip pain*. J. Bone. Joint Surg., 81-B(2), 281-288, 1999.

Demo



Thank you for your attention!